# Optimizing method of mechanism angle of upper limb rehabilitation robot at glenohumeral joint

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Article Info	ABSTRACT
Received Nov 20, 2018	At present, there are seventy million stroke patients in China and annual death toll of stroke is 1 million 650 thousand people. The survivors about 75% become disabled persons and lose the ability to move. To address this issue, a kind of rehabilitation exoskeleton robot called YANARM is proposed which for training of shoulder complex. This paper, a kind of method for optimizing
Keyword:	the angle parameters of series dynamic axes under given workspace conditions is presented. The forward and inverse kinematics solutions of
Optimizing Method Upper Limb Rehabilitation Robot Glenohumeral Joint	glenohumeral mechanism are solved based on the exponential product formula (POE) and the Paden-Kahan sub-problem. The range of joint rotation angle can be inversely solved according to the end of the arm position at the borderline of the workspace. A curve between the angle and the CP which equal mean variance of joint rotation range plus sum of all joint rotation ranges is solved. The mechanism angle of glenohumeral joint is optimized by this method.
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#### 1. Introduction

Post-stroke motor dysfunction is a major problem faced by neurologists. The rehabilitation of the upper limbs of stroke patients has important clinical significance, and the upper limb rehabilitation robot is an important means to solve this problem [1].

Research on upper limb rehabilitation robot began in 1970s [2]. Most of the existing upper limb rehabilitation robots have six or less degrees of freedom. The representative product is the Armeo Power developed by HOCOMA Company [3], which is currently the most widely used upper limb rehabilitation robot in clinical practice. Most of the robots are large to maximize the range of motion of patients 'upper limbs in the rehabilitation process, which affects the selection of motor power to be larger. To optimize the layout of motor in glenohumeral joint and maximize the power-weight ratio of the robot, it is of great significance to the rehabilitation training of shoulder joint by using smaller motor. At present, most rehabilitation robots in the world have orthogonal motor axes in shoulder joint. For example, LIMPACT, an upper limb rehabilitation robot developed by Twente University in the Netherlands [4]. Intelli-Arm, an upper limb rehabilitation robot developed by North-western University [5], and a two-arm rehabilitation robot system developed by Pinole from Italy. Meanwhile a few of robots have considered axis angle of glenohumeral joint motor in design [6]. A MEDARM has been designed by Queen's University of Canada whose shoulder joint structure with small volume [7], however it is very complicated to maintenance and processing for using the rope wheel be the driver. A 7-DOF two-arm rehabilitation robot EXO-UL7 was designed by Washington University, as in [8]. The dynamic considerations were taken into account to reduce the power consumption of the motor, and the trajectory planning and coordinated control of the two arms were carried out. The University of Texas has developed a two-arm rehabilitation robot, Harmony, as shown in Figure 1 from [9]. The axis angle selection of the three motors for the glenohumeral joint ensures that the whole device can still achieve a workspace compatible with the range of human motion in a smaller volume.



Figure 1. Harmony robot

In view of the spherical workspace of 3R series spherical mechanism, this paper presents a method to optimize the angle parameters of series dynamic axes under given workspace conditions.

# 2. Configura Design

# 2.1. The structure and movement mode of shoulder joint

As is known to all, that the human shoulder joint is equivalent to a spherical pair, and the arm mechanism is equivalent to a spherical mechanism which can be selected mainly by a parallel 6R spherical mechanism and a serial 3R spherical mechanism [10], [11]. The working space of the former one is small, and the branches are more likely to interfere with the human body, moreover it requires extremely high and assembly processes to make the three rotating shaft spaces to one point. The other has simple structure and is easy to motion. Combining various factors, this paper chooses serial 3R spherical mechanism as the arm mechanism.

The structure of the mechanism is shown in Figure 2: the shaft  $\$_1$ ,  $\$_2$ , and  $\$_3$  form the upper arm, and the angles between the any two axes of link is  $\alpha$ ; the axis  $\$_4$  controls the motion of the elbow joint, the axis  $\$_5$  controls the axial rotation of the upper arm, and the axis  $\$_6$  controls the motion of the wrist.



Figure 2. 3D model of the structure configuration

The schematic diagram of the mechanism is as shown in Fig.3. The reference coordinate system S and the tool coordinate system T (fixed at the end of the upper arm mechanism) are established, and the coordinate system J (fixed at the rotation centre of the right shoulder joint coincide with S, and the human body faces the negative direction of the Y axis). The three joint axes  $\$_1$ ,  $\$_2$ ,  $\$_3$  intersect at a point S, and the axis  $\$_1$  is

fixed. The angles between the any two axes of link is  $\alpha$ , the length of the upper arm is L, and the joint angle is  $\theta_1$ ,  $\theta_2$ ,  $\theta_3$ .



Figure 3. Schematic diagram of the upper arm mechanism

There are many algorithms in mechanism optimization, as in [12], [13], and [14], in this paper POE and the Paden-Kahan sub-problem used to solve the problem.

When  $\theta_{db} = [\theta_1 \ \theta_2 \ \theta_3]^T = [0 \ 0 \ 0]^T$ , corresponding to the configuration of the upper arm mechanism shown in Figure 6. When  $\theta_{db} = \theta$ , the transformation of the reference coordinate system S and the tool coordinate system T is:

$$\boldsymbol{g}_{st}(\boldsymbol{\theta}) = \begin{bmatrix} \boldsymbol{I} & \begin{bmatrix} \boldsymbol{0} \\ \boldsymbol{0} \\ -\boldsymbol{L} \end{bmatrix} \\ \boldsymbol{0} & \boldsymbol{1} \end{bmatrix}$$
(1)

I is a 3×3 unit array. The coordinates of each motion spin are:

$$\boldsymbol{\xi}_{1} = \begin{pmatrix} c_{\alpha}^{2} & -s_{\alpha}c_{\alpha} & -s_{\alpha} & 0 & 0 & 0 \end{pmatrix}^{T}$$
  
$$\boldsymbol{\xi}_{2} = \begin{pmatrix} c_{\alpha} & -s_{\alpha} & 0 & 0 & 0 & 0 \end{pmatrix}^{T}$$
  
$$\boldsymbol{\xi}_{3} = \begin{pmatrix} 1 & 0 & 0 & 0 & 0 & 0 \end{pmatrix}^{T}$$
  
(2)

The forward kinematics map has the following form:

$$\boldsymbol{g}_{st}\left(\boldsymbol{\theta}_{db}\right) = e^{\xi_{1}\theta_{1}}e^{\xi_{2}\theta_{2}}e^{\xi_{3}\theta_{3}}\boldsymbol{g}_{st}\left(\boldsymbol{\theta}\right)$$
$$= \begin{bmatrix} \boldsymbol{R}\left(\boldsymbol{\theta}_{db}\right) & \boldsymbol{P}\left(\boldsymbol{\theta}_{db}\right) \\ 0 & 1 \end{bmatrix}$$
(3)

### 2.2. Inverse kinematics

Let Eqs. (3) be equal to  $g_d$ :

$$\boldsymbol{g}_{st}(\boldsymbol{\theta}_{db}) = e^{\hat{\xi}_{1}\theta_{1}} e^{\hat{\xi}_{2}\theta_{2}} e^{\hat{\xi}_{3}\theta_{3}} \boldsymbol{g}_{st}(\boldsymbol{\theta}) = \boldsymbol{g}_{d}$$

$$\tag{4}$$

In Eqs. (4),  $g_d \in SE(3)$  is the desired shape of the tool coordinate system T, also the desired shape of the upper arm. Eqs. (4) left multiply  $g_{st}^{-1}(\theta)$  to get exponential mapping

$$e^{\hat{\xi}_1\theta_1}e^{\hat{\xi}_2\theta_2}e^{\hat{\xi}_3\theta_3} = \boldsymbol{g}_d\boldsymbol{g}_{st}^{-1}(\boldsymbol{\theta}) = \boldsymbol{G}_1$$
(5)

First step (solving  $\theta_1$  and  $\theta_2$ ): applying both sides of Eqs. (5) to the point  $P_3 \in R(3)$  on axis  $\$_3$  (but the point is not on the axis  $\$_1$  and  $\$_2$ ). Because of  $e^{\hat{\$}_3 \theta_3} P_3 = P_3$ , so:

$$e^{\hat{\xi}_1\theta_1}e^{\hat{\xi}_2\theta_2}\boldsymbol{P}_3 = \boldsymbol{G}_1\boldsymbol{P}_3 \tag{6}$$

The above equation conforms to the form of the Paden-kahan sub-question 2. In Eqs. (6),  $P = P_3$   $Q = G_1P_3$ ,  $\theta_1$  and  $\theta_2$  can be solved.

Second step (solving  $\theta_3$ ): since  $\theta_1$  and  $\theta_2$  are known, Eqs. (5) can be transformed into:

$$e^{\hat{\xi}_3\theta_3} = e^{-\hat{\xi}_2\theta_2} e^{-\hat{\xi}_1\theta_1} \boldsymbol{G}_1 \tag{7}$$

Applying both sides of Eqs. (7) to the point  $P_2 \in R(3)$  on axis  $\$_2$  (but not at axis  $\$_1$  and  $\$_3$ ):

$$e^{\hat{\xi}_3\theta_3}\boldsymbol{P}_2 = e^{-\hat{\xi}_2\theta_2}e^{-\hat{\xi}_1\theta_1}\boldsymbol{G}_1\boldsymbol{P}_2 \tag{8}$$

The above equation conforms to the form of the Paden-kahan sub-question 1. In Eqs.(8),  $P = P_2 \quad Q = e^{-\hat{\xi}_2 \theta_2} e^{-\hat{\xi}_1 \theta_1} G_1 P_2$ ,  $\theta_3$  can be solved.

### 3. Mechanism Parameter Optinization

In order to get more rang of motion (ROM) of shoulder, it is necessary to optimize the mechanism angle. In [15], Luige's research on robotic haptic sense points out the direction for the follow-up study of this paper. Since S and J coincide, the representation of the four extreme poses of the human body in the coordinate system J is the same as the pose of the tool coordinate system T under the reference coordinate system S: Substituting  $g_{dA}$ ,  $g_{dB}$ ,  $g_{dC}$ , and  $g_{dD}$  into Eqs. (4) respectively, the value of  $\theta_1$ ,  $\theta_2$ , and  $\theta_3$  can be solved according to the inverse solution algorithm. Each extreme pose can solve two sets of inverse solutions, and

each group of inverse solutions corresponding to each of the four extreme positions can get a combination. There are 16 cases, for each case can get a range of  $\theta_1$ ,  $\theta_2$ , and  $\theta_3$  values.

Define  $AR_{op} = fw_1 + fw_2 + fw_3 + st_{123}$  as the angle indicator. When  $AR_{op}$  is minimum, the total rotation range of the three rotation pairs is small, and the distribution on the three rotation pairs is relatively uniform.

When  $AR_{op}$  is the smallest, the corresponding combination is the optimal combination, and the range of values of the three angles corresponding to the combination is selected. Where  $fw_i$  is the range of values for  $\theta_i$  and  $st_{123}$  is the mean square of the range of values for the three angles. The relationship between  $\alpha$  and  $AR_{op}$  is shown in Figure 4.

Known from Figure 4,  $AR_{op} = 433^{\circ}$  is the minimum value when  $\alpha = 72^{\circ}$ . When  $\alpha = 72^{\circ}$ , it is the optimal solution.

When  $\alpha = 72^{\circ}$  and  $AR_{op}$  smallest corresponding arrangement, obtain  $\theta_1 \in (-58, 123)$ ,  $\theta_2 \in (-142, 15)$ ,  $\theta_3 \in (-96, 0)$ . Substituting them into the positive solution equation, we got the positional relationship



between the arc path and the spherical area of the point ( $P_2$  and  $P_3$ ), and the human body area, as shown in Fig. 5.

Figure 4. Relationship between  $\alpha$  and  $AR_{an}$ 



Figure 5. Intervention between the mechanism and human body

# 4. Conclusion

By defining the angle index, the angle of the mechanism linkage is globally optimized, so that the total rotation range of the three rotation pairs is small, and the distribution on the three rotation pairs is relatively uniform.

By defining the distance parameter JL, performing global optimization from the two dimensions  $\beta_1$  and  $\beta_2$ . The obtained pose parameters can effectively avoid the interference between the mechanism and the human body.

The internal and external rotation degrees of the end link are artificially fixed, that is, the same internal and external rotation angles are used for multiple extreme positions. When different internal and external rotation angles are taken, different optimization results are obtained, and the subsequent relationship will be further studied.

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## References

- [1] Gu T, Li CJ, Zhan Q (2017) Advances in application of rehabilitation robots for upper limb dysfunction in patients with stroke. In "J Neurol Neurorehabil," 13(1):44-50.
- [2] Winklevoss HE (1974) Inflation based variable life insurance models. in "J Risk Insur," 41(4):601-619.
- [3] Tobias N, Marco G, Robert R (2009) ARMin III- arm therapy exoskeleton with an ergonomic shoulder actuation. in "Applied Bionics and Biomechanics," 6(2):127-142.
- [4] Otten A, Voort C, et al. (2015) LIMPACT: a hydraulically powered self-aligning upper limb exoskeleton. in "IEEE/ASME Transactions on Mechatronics," 20(5): 2285-2298.
- [5] Ren Y, Park H S, et al.(2009) Developing a whole-arm exoskeleton robot with hand opening and closing mechanism for upper limb stroke rehabilitation. in "IEEE International Conference on Rehabilitation Robotics," Tokyo, Japan, 761-765.
- [6] Pignolo L, Dolce G, et al.(2012) Upper limb rehabilitation after stroke: ARAMIS a "robo-mechatronic" innovative approach and prototype. in "IEEE Ras & Embs International Conference on Biomedical Robotics and Biomechatronics," Rome, Italy, 1410-1414.
- [7] Ball S J, Brown I E, et al.(2007) MEDARM: a rehabilitation robot with 5DOF at the shoulder complex. in "IEEE/ASME International Conference on Advanced Intelligent Mechatronics," Zurich, Switzerland, 1-6.
- [8] Yu W, Rosen J.(2010) A novel linear PID controller for an upper limb exoskeleton. in "IEEE Conference on Decision and Control," Atlanta, USA, 3548-3553.
- [9] Kim B, Deshpande A D, et al.(2017) An upper-body rehabilitation exoskeleton Harmony with an anatomical shoulder mechanism: Design, modeling, control, and performance evaluation. in "International Journal of Robotics Research," 36(4): 414-435.
- [10] Zhang LJ, Zong JF. (2000) Research on Workspace of Spherical 3-DOF Series Robot. in "Chinese Jouranal of Mechanical Engineering," 36(10):104-107.
- [11] Liu FY, Yang XS. (2010) Advances and Trends in Spherical Mechanisms Research. in "Machine Design and Research," 26(1):32-35.
- [12] Wang XJ, Wang XY, et al. (2014) Dynamic analysis for the leg mechanism of a wheel-leg hybrid rescue robot. in "IEEE International Conference on Control," Loughborough, UK, 504-508.
- [13] Ion I, Vladareanu L, et al. (2007) The improvement of structural and real time control performances for MERO modular. in "Advances in Climbing and Walking Robots," 252-263.
- [14] Vladareanu L, Curaj A, et al. (2012) Complex Walking Robot Kinematics Analysis And Plc Multi-Tasking Control. in "Rev. Roum. Sci. Techn. - Électrotechn. et Énerg, 57 (1): 90-99.
- [15] Luige V, Octavian M, et al. (2014) Haptic interfaces for the rescue walking robots motion in the disaster areas. in "IEEE International Conference on Control," Loughborough, UK, 498-503.

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